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Interface and display of Electromyography signal wireless measurements

Kevin Eka Pramudita¹

¹Electrical Engineering
Department Soegijapranata
Catholic University
Paviyatan Lubuk IV/1 Bendan
Dewar 50234, Semarang,
Indonesia
keveto7@yahoo.com

F.Budi Setiawan²

²Electrical Engineering
Department Soegijapranata
Catholic University
Paviyatan Lubuk IV/1 Bendan
Dewar 50234, Semarang,
Indonesia
fbudisetiawan@yahoo.com

Siswanto³

³Psychology Department
Soegijapranata Catholic
University
Paviyatan Lubuk IV/1 Bendan
Dewar 50234, Semarang,
Indonesia
tissles@yahoo.com

Abstract- This paper had explained an interface and display system of Electromyography signal results from wireless measurements method. The interface by using bluetooth as connection from Electromyography measurement device which used to measure human skeletal muscle activities. Electromyography device display results from human skeletal muscle measurement. The results would be transferred by bluetooth to displayed in gadget application (e.g. notebook, smartphone, tablet, netbook, etc.). The application we were used is Virtual Analyzer on Windows operating system and AED in Android operating system. The use of two application is intended that the results of electromyography signal could be seen and accessed on most operational system platform which used by gadgets. Finally, after wireless interface and the display of Electromyography signal had been described, then conducted experimental measurements toward 10 people in two difference parts of body for example shoulder and stomach. There were sample and proof that human muscle generates electricity when strained or contracted.

Key words: Electromyography signal, interface, display, measurements

1. INTRODUCTION

In the era of rapid development of technology has great influence in the development of electrophysiology as a part from biomedical world, especially on Electromyography (EMG). That influence has changed the system of electromyography device become simpler than before.

Electromyography signal is a biomedical signal that is obtained via electrical response generated in muscles during its contraction representing neuromuscular activities.[1] To obtain a good results of EMG measurements there are several steps that must be considered especially the measurements step was important one to attention, commonly surface EMG method is the common method of measurement[2].

The usage of wireless measurement interface is based on variety of benefits that have been obtained[3], in this case bluetooth as the connection between Electromyography measurements device and the viewer gadget of electromyography signal measurement results. The main benefit is

2.0 connection could eliminate the disadvantages owned by cable connection/interfaces[3].

Windows and Android were selected as application display of EMG signal measurement results because both of them is the operating system mostly used in gadgets (Windows had 95% marketshare in PC, Notebook, Netbook operating system, while Android had 62.6% marketshare in tablet and smartphone)[4][5]. On the experiments that have been done, we used the PA/Virtual Analyzer application for Windows operating system platform and AED(Android Electromyograph Display) application for Android operating system platform.

We have conducted experiments of electromyography signal measurements of several parts of the body muscles with the used of electromyography measurements device that has been made to saw the electrical signals that can be produced by body muscles when contracted.

II. RESEARCH METHODS

2.1 Electromyography

Electromyography (EMG) is a method in experimental technique used to record electric signal which produced by human muscle fiber.[6] Electromyography is used to measure the electrical activity generated by movement of substances Na^+ and K^+ inside body muscle tissue[7]. There are two methods of EMG measurements: surface measurements and intramuscular measurements, we have chosen the method of surface measurements on the experiments we have done with the reason that the measurements on the skin surface of the subject, can be conducted by personnel other than medical Doctors, with minimal risk to the subject.[2]. Therefore the measurement steps must be considered, such as skin preparation for measurements and the electrode unit, the preparation of the skin surface prior to measurement by eliminating obstacles such as skin hair, sweat, bacteria, etc. These obstacles can be removed by the use of abrasive cleaning paste, soft sand paper, and alcohol[2]. Then

an electrode itself as considered an electrode consisted a highly conductive metal, silver, interface to its salt, silver chloride. Silver-silver chloride based electrode design is known to produce the lowest and most stable common potentials[6]. This electrode is shown on figure 1 produced by Biomed manufacturer.



Fig. 1. Silver-silver chloride based EMG electrodes (on the left side is solid form and on the right side is gel form)

2. Electromyography measurement devices

The Electromyography measurements that had been made, operate in a way, the input signal from EMG surface measurements amplified by AD 620 IC, an operational amplifier with a gain value of the input was 1000 times after the EMG signal is amplified by 1000x, the signal was then amplified again through AD 620 IC with the use of cermet as a regulator of the signal gathering in order to smoothing the ripples present in the signal wave, resulting from the use of AD 620 IC, so the EMG signal measurement results can look more refined. Both of these found in the Electromyography measurement device as the pre-amplifier and supplied by 2x9v batteries and the power supply already regulated by the device as required by IC. The input signal must be amplified because the actual input signal from the EMG surface measurements typically from a few µV to over peak to peak[8][9]. The EMG recording should not use any hardware filters (e.g. notch filters) because EMG has large signal contributions at these frequencies. The result of notch filtering is the loss of important EMG signal information, so much filtering should be avoided as a general rule[7].

The figure 2 shows EMG measurements device that we made unit that we had made



Fig. 2. EMG measurements device

On figure 2 above described about parts inside Electromyograph measurements device ,for further explanation of the entire process of EMG measurements from electrode unit to the display application unit , described as block diagram process is figure 3

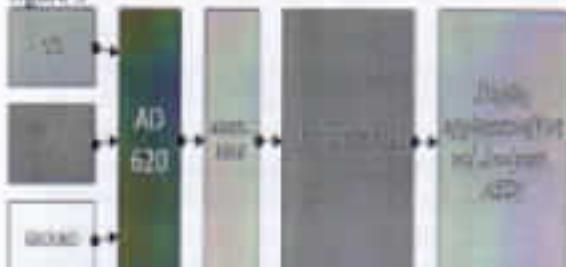


Fig. 3. Electromyograph measurements block diagram

On the figure 2 above V1,V2 and ground as the electrode , and the AD 620 as the amplifier to amplified input signal before passed to the filter and then transferred by bluetooth in wireless interface to showed in the display application(TMS320F2812).

2.3. Wireless interface measurements

Wireless interface was selected as the connection between the measurements unit and the display unit because this interface had many advantages over cable interface as thought wireless interface already had it's own network so without any interference with other networks, then low power transmission needs so can longer life of the device power supply and the time used to perform measurements[10]. Bluetooth 2.0(A2DP/Advanced Audio Distribution Profile) were selected as wireless interface due to the reasons that have been presented above, plus the advantages of A2DP networks that can connect a wide range of electronic hardware without specific programming [11]Figure 4 shown Bluetooth 2.0 device that is used as a wireless interface



Fig. 4. Bluetooth2.0
(A2DP/AdvancedAudioDistributionProfile) headset

2.4 Display unit.

The display unit using *Virtual Analyzer* application has function in addition to the main function is to show electromyography signal measurement results, so that can be read easily by nonmedical person. *Virtual Analyzer* also can filtering the EMG signal measurement results by using the digital filter, in EMG signal processing, band pass filter and high pass filter is selected, the band pass filter is selected because the EMG signal frequency is dominant in 30-500Hz bandwidth frequency spectrum, and then high pass filter is used in order to remove DC noise because any difference in the D/C potential measured at the each of the electrode sensors will be amplified, which can lead to pre-amplifier instability or saturation [9]. In figure 5 would be shown menu to select the digital filter option provided by *Virtual Analyzer* application.



Figure 5. *Virtual Analyzer* digital filter option menu

After the digital filter option is set, then the EMG signal measurement results can look more refined, the figure 6 shown *Virtual Analyzer* display application that runs on the Windows operating system platform,

the *Virtual Analyzer* was displaying EMG signal when body muscle relaxed.

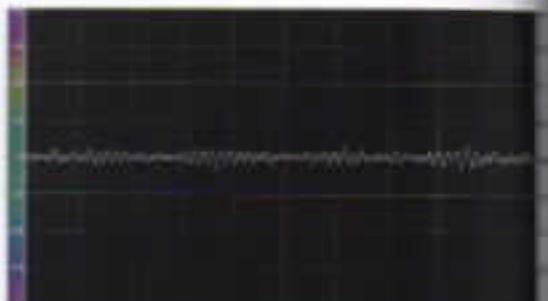


Figure 6. *Virtual Analyzer* displaying body muscle when relaxed

And on the figure 7 shown *Virtual Analyzer* display application was displaying EMG signal when body muscle contracted.

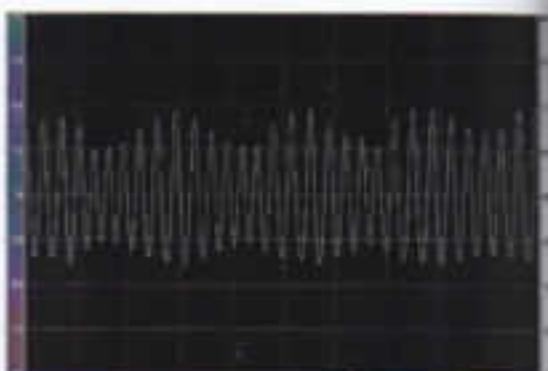


Figure 7. *Virtual Analyzer* displaying body muscle when contracted

EMG signal measurement results are also displayed on AED display application that runs on the Android operating system platform, in figure 8, shown AED display application displaying body muscle when relaxed.

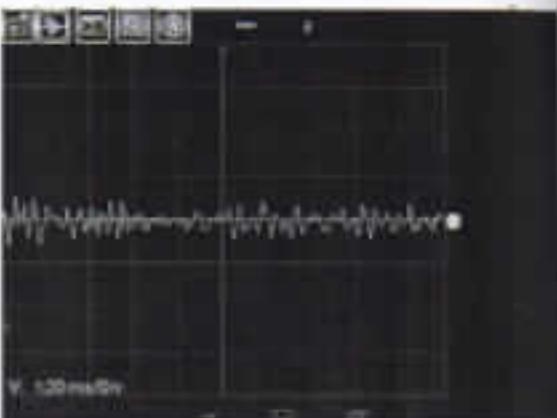


Figure 8. AED displaying body muscle when relaxed

Then, the figure 9, shown AED display application displaying body muscle when contracted



Figure 9. AED displaying body muscle when contracted

III. EXPERIMENTAL RESULTS

Based on the various of research methodologies is has been described in the previous chapter, we conducted experiments measuring an electromyographic signal, as in figure 9 shown on electromyograph measurements experiments that have been carried out by the method skin surface of the body measurements, first in figure 9 EMG measurement measurements conducted on shoulder skin's surface with the electrode placement configurations



Fig. 10. EMG measurements on shoulders skin surface

Then in figure 10 is shown the experimental measurements performed on the stomach skin surface, with electrode placement configurations



Figure 11. EMG measurements on stomach skin surface

From figures 9 and 10 are shown above, the EMG measurement experiment performed on the two parts of the body to the 10 participants in our department, the table 1 shown the results of Electromyography experimental measurement

Table 1. Results of Electromyography experimental measurement

Row	Number	Electromyography signal voltage measurement results in V			
		Relaxation	Contracted	Relaxation	Contracted
1	Participant 1	0.2	0.3	5.8	2.6
2	Participant 2	0.3	1	3.1	3.6
3	Participant 3	0.15	0.8	1	0.6
4	Participant 4	0.2	0.4	3.3	2.4
5	Participant 5	0.35	0.65	3.8	3.3
6	Participant 6	0.3	0.2	3.3	1.6
7	Participant 7	0.6	1.7	3.05	3.05
8	Participant 8	0.2	1.8	3.2	1
9	Participant 9	0.25	1	3.6	1.4
10	Participant 10	0.25	0.6	1	1

From the measurement results in the table 1 above, is influenced by various factors on the surface of the skin condition participant fat thickness, impedance, muscle fatigue, etc. Experimental results of the EMG measurements is calculated by measuring the difference between the highest peaks and the lowest valleys of the wave signal measurement results are displayed by Virtual Analyzer or AED display application. Calculation of this EMG signal measurement results, based on a variety of reference that have been searched and the research that has been done [2][7][8][9][12]. The figure 11 and 12 are shown the highest peak and lowest valley of the EMG signal measurement results, when the muscle relaxed (Fig. 11) and the muscle contracted (Fig. 12).

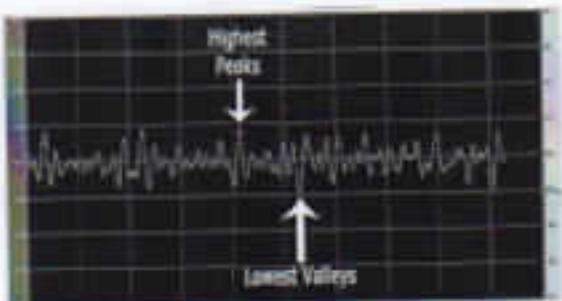


Fig. 12. the highest peaks and the lowest valleys of EMG signal measurement results when the muscle relaxed

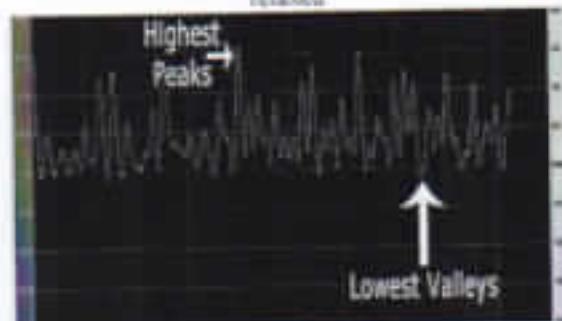


Fig. 13. The highest peaks and the lowest valleys of EMG signal measurement results when the muscle contracted

IV. CONCLUSION

From the results of experiments that have been conducted, it can be concluded that the EMG signal measurement results have an average value of the difference between relaxation and contraction is greater, when the EMG measurements were done on the shoulders of the participant compared with the average value of the measurement signal on the stomach, it is proposed to prepare it beforehand the various steps that must be considered before the EMG measurements performed, such as on the electrode, the condition of the skin surface of the body and the condition of EMG measurement device to get a good measurement result.

V. ACKNOWLEDGEMENTS

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VI. REFERENCES

- [1] Faiz, Sharif, A., Iqbal, Md. Asif, Junaid, M. Ahmed, Jidduwah, A. B. M. Sayed, Identifying the Major Neurotransmitter in EMG Signal using Time and Frequency Domain Features with Computer, SPU, Bangladesh April 2012
- [2] Dey, Dr. Scott, Important factors in surface EMG measurements, Biorad Biomedical Ltd, Calgary 2004
- [3] Tuncer, J. Dibbagh, McGrath, Michael, Kam, Ben, Wireless Sensor Networks for Healthcare Applications, ArtechHouse, Norwood, USA 2010
- [4] Venkat, Murthy, Enhanced Discovering Computer Fundamentals, Your Interactive Guide to the Internet, USA 2012
- [5] Miller, Rebecca R., Mortfield-Lang, Heather, Menz, Carolyn, Tablet Computers in the Academic Library, ALA Edition, Virginia 2014
- [6] Shakir, Naseeb V., Biopotentials and Electrophysiology Measurement, CRC Press LLC, Canada 2000
- [7] C.J. De Luca, M. Knutson, Surface Electromyography: What's New? CLUTT Toronto 1992
- [8] J.V. Basmajian, C.J. De Luca Muscle Alive: Their Function revealed by Electromyography, William Wilkins, Baltimore 1985
- [9] Konrad-Preis, The ABC of EMG : A Practical Introduction to Kinanthropological Electromyography, April 2005
- [10] Prasad, Ranjeev, Milivojka, Alena, New Horizons in Mobile and Wireless Communication Networks, services and applications, ArtechHouse, Norwood, USA 2009
- [11] Na-in-Sik, Suck-Jin, Seo, Sung-Min, Chang-Hwan, Park, Hyun-Jae, Hwang, Sung-Jae, Schmid, Manu, Thomas, Braden, Tedrew, Protopsaltis, Michael, and Rolf, Rassner, "Clinical Technologies Concepts, Methodologies, Tools, and Applications", Information Resources Management Association, Chap.3.23, pp.974-1075, 2011
- [12] Ibernie, A., Butler, R., Simultaneous measurement of muscle contraction, velocity and EMG power spectrum changes during fatigue. *Muscle & Nerve*, 8, 768-773, 1985

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Dean of Faculty Engineering, Diponegoro University

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